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Development and *Invitro* Evaluation of Azithromycin Microspheres by Solvent Evaporation Technique

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Article info

Abstract

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Keywords: Azithromycin, Microspheres, Ethyl cellulose, Solvent evaporation. The present investigation was concerned with formulation and evaluation of microspheres for Azithromycin using Ethyl cellulose as a release retarded material by solvent evaporation technique. Nine different batches of Microspheres were prepared using three different solvents at three different Drug: polymer ratios (1:1, 1:1.5, 1:2) The microspheres were characterized for drug content, percentage yield, particle size analysis and surface morphology. The results of all the physiochemical tests of all formulations were found to be favorable. The invitro % drug release was found to be in range of 59.13 to 80.13 %. At the end of 12 hrs. Optimized formulation C3 was evaluated for FTIR, XRD and SEM. XRD and FTIR studies showed that the nature of pure drug Azithromycin remains unaffected till the completion of process of microspheres formation. SEM photographs showed that the Floating microsphere. The in vitro data were fitted to different Kinetic order. The formulated tablets exhibited Fickian to anomalous transport drug release thenetics approaching Zero–order as the value of release rate exponent (n) varied between 0.524 to 0.784.

1. INTRODUCTION

Microencapsulation is a process whereby relatively thin coating of polymers are applied to small particles of solid or droplets of liquid and dispersions. The microencapsulation processes produce small particles ranging in size from 1 to 1000 µm. microcapsules are made of one or multiple core substances (solid or liquid) that are surrounded by a distinct capsule wall, whereas micromatrices are polymeric matrices in which the encapsulated substances are homogeneously dispersed^{1,2}. Azithromycin is a macrolide antibiotic that has been used for more than a decade to treat urinary tract, bronchial tract, lungs and sinuses infections. The unique pharmacokinetics of Azithromycin-rapid absorption and extensive distribution in tissue allows for short 3-day (500 mg/day for 3 days) or 5-day (500 mg on day 1 followed by 250 mg on day 2-5) course of therapy. Preclinical studies have shown that Azithromycin efficacy related to AUC//MIC ratio that improved efficacy could result if the therapeutic courses were given all at once as single dose.

Azithromycin when incorporated into sustained release microspheres, release the drug slowly. And the drug is released into the lower gastrointestinal tract, reducing gastrointestinal side-effects, and allowing for a higher dose to be administered. The unique pharmacological properties and extremely long half-life of Azithromycin make this drug well suited to single-dose administration. Azithromycin dihydrate is insoluble in water and also bitter taste by making in microsphere formulation taste masking can be done, so fast onset of action achieved and potential for avoidance of hepatic first pass metabolism of susceptible drug and causes increase in the bioavailability.

Azithromycin has low bioavailability also having large dose which may cause GI side effect hence, by making in sustained release form it will released in lower GI tract and minimizes side effect. Aim of this study was an attempt taken for preparation of sustained released microspheres using ethyl cellulose, which will reduce the dosing frequency³.

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2. MATERIALS AND METHODS

Azithromycin and Ethyl cellulose (50 cps) was obtained as gift sample by Zim Laboratories Ltd, Nagpur (Maharashtra) India. All other materials and solvents used were of analytical grade.

2.1 Formulation of Microspheres

The formulations were prepared by using different solvents (ethyl acetate dichloromethane, chloroform) and different drug: polymer ratio (1:1, 1:1.5, 1:2) in each solvent. In the O/W emulsion solvent evaporation method, the polymer (ethyl cellulose) was dissolved in internal organic phase or solvent. Accurately weighed quantity 1g of Azithromycin was dispersed or dissolved in the polymer solution. This resulting mixture was poured slowly with stirring into 100 ml of a 0.015% w/v aqueous solution of polyvinyl alcohol. The emulsion was then stirred continuously at 700 rpm for 1 hr to evaporate the solvent. The microspheres were recovered by vacuum filtration, washed with 200 ml of deionized water and dried at room temperature^{4, 5}.

S. No.	Formulation code	Drug : Polymer Ratio	Internal Organic Phase	
1	A1	1:1		
2	A2	1:1.5	Chloroform	
3	A3	1:2		
4	B1	1:1		
5	B2	1:1.5	Dichloromethane	
6	B3	1:2		
7	C1	1:1		
8	C2	1:1.5	Ethyl Acetate	
9	C3	1:2		

2.2 Evaluation of Microspheres

2.2.1 Angle of Repose

Angle of repose is defined as the maximum angle possible between the surface of pile of powder and horizontal plane. The angle of repose for the microspheres of each formulation was determined by the funnel method⁶. The microspheres were allowed to flow out of

the funnel orifice on a plane paper kept on the horizontal surface. It forms a pile of microspheres on the paper. The angle of repose was calculated by substituting the values of the base radius 'R' and pile height 'H' in the following equation

 $Tan \theta = H/R$

Where, H = Pile Height. R = Radius of Pile.

2.2.2 Bulk Density

Bulk density of all batches of microspheres was determined by pouring gently 2 g of sample through a glass funnel into a 10 ml graduated cylinder. The volume occupied by the sample was recorded. Bulk density was calculated as per given formula:

Weight of sample

Volume occupied by the sample

2.2.3 Tapped Density

Bulk density =

The tapped density was determined by pouring 2 g of microspheres through a glass funnel into a 10 ml graduated cylinder. The cylinder was tapped from height of 2 inches until a constant volume was obtained. Volume occupied by the sample after tapping was recorded .The values for tapped density was calculated as per given formula:

Tapped density (g/ml) = Volume occupied by the sample

2.2.4 Compressibility Index

The compressibility indices of the formulation blends were determined using Carr's compressibility index formula. Tapped density – Bulk density

Carr's Index =

----- X 100 Taped density

2.2.5 Hausners Ratio

It provides an indication of the degree of densification which could result from vibration of feed hopper. Lower the Hausner ratio better is the flowability. It was calculated as per given formula.

Hausner ratio = Tapped density Bulk density

2.2.6 Determination of Particle Size

The particle size was determined using stage micrometer. The diameters of about 300 microspheres were measured and the average particle size was determined⁷.

2.2.7 Estimation of Drug Loading

For determination of drug content, microspheres equivalent to 100 mg were weighed and dissolved in 100ml of acetone. After suitable dilutions were with phosphate buffer (pH 6.0), the resulting solution was analysed spectrophotometrically at 244 nm^{8,9}.

Actual drug content

Encapsulation efficiency (%) = ------ × 100 Theoretical drug content

Weight of drug

Weight of microspheres

% Yield = ------ × 100 Total expected weight of drug and polymer

2.2.8 In-vitro Dissolution Study

Accurately weighed microspheres equivalent to 200 mg of Azithromycin were taken in muslin cloth and it was kept in baskets. Dissolution study was carried out in phosphate buffer pH 6.0 at 50 rpm at temp 37 ± 0.5 °c. During dissolution study 10 ml of aliquot was withdrawn at a time intervals of 1 to 12 hr and same was replaced with equal volume of fresh medium. The withdrawn samples were filtered through Whatmann filter paper and

absorbances were measured at 244 nm. Drug concentration in the samples was determined from the calibration ${\rm curve}^{10}$.

2.3 Characterization of Microspheres

2.3.1 Differential Scanning Calorimetry

The DSC measurements were performed on a differential scanning colorimeter with thermal analyzer. All accurately weighed samples (about 10 mg of Azithromycin, ethyl cellulose, physical mixtures, and formulation) were placed in sealed aluminium pans, before heating under nitrogen flow (10 ml/min) at a scanning rate of 20 c per min from 100 to 300 c an empty aluminum pan was used as reference^{12,13}.

2.3.2 X-Ray Diffractometry

The powder X-ray diffraction pattern of Azithromycin and polymer were obtained using Phillips X-ray diffractometer with a Ni-filtered CuK α -radiation at a scanning speed of 10 ° [/]min at 20.The graph was plotted in 2 theta angle versus intensity count¹⁴.

2.3.3 Surface Morphology

The microspheres were coated with Platinum by ion sputtering using Autofine coater. The microspheres were kept on the sample holder and the scanning electron micrographs were taken¹⁵.

2.3.4 Stability studies

The optimized formulation was subjected to study the effect of temperature. The study was carried out by storing the microspheres in glass bottle 40° C± 2° C and 75%±5% RH for 30 days. These samples were collected on 7th, 14th, 21st, 28th day and analyzed for changes drug content and *in-vitro* dissolution studies¹⁸.

2.3.5 Kinetic Treatment to Dissolution Data

The dissolution data for all formulations was fitted to various drug release kinetic models like Zero order, First order, Higuchi Matrix and Korsemeyer Peppas, Hixon-Crowel model. Rate constants (K), correlation coefficients (R) obtained for various models. And Release exponent (n) values obtained in Korsemeyer Peppas model was studied^{16, 17, 19}.

3. RESULTS AND DISCUSSION

IR spectra for Azithromycin, ethyl cellulose and physical mixture of Azithromycin and ethyl cellulose are given in fig.1-3. Major functional groups of Azithromycin (CH₃-N Stretching) at 1377, (CH₂ Scissoring) at 1454, (C=O stretching) at 1720, (COOH) at 2891, (C-H Stretching of methyl and methylene) 2912, (O-H Stretching Vibration) at 3560 can be seen in spectra of individual drugs as well as in spectra of physical mixture. So there is no interaction between Azithromycin and ethyl cellulose.





Figure-2: IR spectrum of Ethyl cellulose



Figure-3: Azithromycin + Ethyl cellulose

All the formulations show angle of repose value in the range of 15.22 - 20.42. The values for bulk density were found in the range of 0.333 to 0.455. Tapped density was found to range from 0.380 to 0.536. Compressibility index were found in the range of 11.76 to 15.11 respectively. Hausner's ratio was ranging from 1.13 to 1.17, i.e., all the preparation showed that they had good flow properties.

Angle of Repose (θ)	Bulk Density (g/ml)	Tapped Density (g/ml)	Carr's Compressibility Index (%)	Hausner's Ratio
16.19±0.754	0.429±0.039	0.504±0.064	14.88±0.024	1.17±0.0675
15.22±0.534	0.405±0.024	0.462±0.036	12.33±0.032	1.14±0.064
15.51±0.633	0.391±0.024	0.445±0.014	12.13±0.075	1.13±0.023
17.19±0.644	0.423±0.035	0.490±0.064	13.67±0.075	1.15±0.046
18.36±0.352	0.333±0.063	0.380±0.047	12.36±0.035	1.14±0.067
19.41±0.656	0.455±0.062	0.536±0.024	15.11±0.013	1.17±0.045
19.72±0.353	0.352±0.044	0.414±0.042	14.97±0.064	1.17±0.025
20.38±0.755	0.431±0.023	0.507±0.045	14.99±0.034	1.17±0.052
20.42±0.353	0.450±0.035	0.510±0.074	11.76±0.042	1.13±0.025
	Angle of Repose (θ) 16.19±0.754 15.22±0.534 15.51±0.633 17.19±0.644 18.36±0.352 19.41±0.656 19.72±0.353 20.38±0.755 20.42±0.353	Angle of Repose (θ) Bulk Density (g/ml) 16.19±0.754 0.429±0.039 15.22±0.534 0.405±0.024 15.51±0.633 0.391±0.024 17.19±0.644 0.423±0.035 18.36±0.352 0.333±0.063 19.41±0.656 0.455±0.062 19.72±0.353 0.352±0.044 20.38±0.755 0.431±0.023 20.42±0.353 0.450±0.035	Bulk Density (g/ml) Tapped Density (g/ml) 16.19±0.754 0.429±0.039 0.504±0.064 15.22±0.534 0.405±0.024 0.462±0.036 15.51±0.633 0.391±0.024 0.445±0.014 17.19±0.644 0.423±0.035 0.490±0.064 18.36±0.352 0.333±0.063 0.380±0.047 19.41±0.656 0.455±0.062 0.536±0.024 19.72±0.353 0.352±0.044 0.414±0.042 20.38±0.755 0.431±0.023 0.507±0.045	Angle of Repose (θ) Bulk Density (g/ml) Tapped Density (g/ml) Carr's Compressibility Index (%) 16.19±0.754 0.429±0.039 0.504±0.064 14.88±0.024 15.22±0.534 0.405±0.024 0.462±0.036 12.33±0.032 15.51±0.633 0.391±0.024 0.445±0.014 12.13±0.075 17.19±0.644 0.423±0.035 0.490±0.064 13.67±0.075 18.36±0.352 0.333±0.063 0.380±0.047 12.36±0.035 19.41±0.656 0.455±0.062 0.536±0.024 15.11±0.013 19.72±0.353 0.332±0.044 0.414±0.042 14.97±0.064 20.38±0.755 0.431±0.023 0.507±0.045 14.99±0.034 20.42±0.353 0.450±0.035 0.510±0.074 11.76±0.042

 Table 2: Physical parameters of Azithromycin Microsphere

As the polymer concentration increases, viscosity also increases which influences the interaction between disperse phase and dispersion medium that affects the size distribution of particle. Result indicated that increase in the amount of polymer concentration increases relative viscosity which results into increased mean particle size. The average particle size of microcapsules is found to be within 112.546 to 171.342 μ m.Results were given in figure 4.



Figure-4: Graphical presentation of average particle size

The percent encapsulation efficiency of ethyl cellulose microsphere shown in table 3. The drug: polymer ratio showed significant effect on the encapsulation efficiency of microsphere. The increase in concentration of polymer showed the increase in drug encapsulation efficiency. The microsphere formulated using ethyl acetate as internal organic phase or solvent showed better encapsulation efficiency than other formulations. The % encapsulation efficiency is found to be in the range of 63.61 ± 0.7 to 75.60 ± 1.32 %.

From the *in vitro* drug release study it can be seen that the C1 batch showed sustained cumulative % drug release 80.13% in 12 hrs. Although formulation A3 showed cumulative % drug release of 59.13 % in 12 hrs and formulation B3 showed cumulative % drug release of in 67.18 % in 12 hrs, their release was insufficient. As the polymer concentration increased the drug release was decreased. The batches of microsphere formulated using ethyl acetate as solvent showed higher release rate than other solvents. The batches of microsphere formulated with drug: polymer ratio 1:1 showed higher release rate than other ratios. Results were Given in figure 5.

 Table 3: Data for Percentage yield, percentage loading and encapsulation efficiency of microspheres

Formulation Code	Drug : Polymer	Theoretical loading (%)	Actual Drug Loading (%)	Encapsulation Efficiency (%)	Yield (%)
A1	1:1	50	52.16 ± 0.905	64.48 ± 1.81	95.85
A2	1:1.5	40	45.02 ± 0.455	65.76 ± 1.13	87.68
A3	1:2	33.33	34.42 ± 0.355	66.25 ± 1.06	96.83
B1	1:1	50	51.89 ± 0.35	63.61 ± 0.7	96.35
B2	1:1.5	40	45.02 ± 0.45	64.76± 1.13	88.84
B3	1:2	33.33	34.34 ± 0.44	64.82 ± 1.33	97.23
C1	1:1	50	52.08 ± 0.202	74.40± 0.405	96.0
C2	1:1.5	40	44.44 ± 0.53	75.60 ± 1.32	90.0
C3	1:2	33.33	34.47 ± 0.38	73.50 ± 1.14	96.34
n = 3					



Figure-5: % Cumulative drug release of microspheres

The dissolution data for formulations A1, A2, A3, B1, B2, B3, C1, C2, and C3 was fitted to various drug release kinetic models like Zero order, First order, Higuchi Matrix and Korsemeyer Peppas, Hixon-Crowel model. Rate constants (K), correlation coefficients (R) obtained for various models are listed in table 4.with Release exponent (n) values obtained in Korsemeyer Peppas model .The model that gives high 'R' value is considered as the best fit model for the release data. It was found that as Korsemeyer Peppas best fit model for all the formulations tested. All the formulations showed

diffusion exponent (n) varying from 0.524 to 0.784. From the n values of all formulations it can be concluded that as the concentration and viscosity of polymer was increased the value of diffusion exponent also increases. This was because as the concentration of polymer increases, the rate of dissolution of disentangled chains decreases and diffusion path length of

aqueous channel increases. This leads to increase in diffusion exponent value and results in shifting of the mechanism of drug release from fickian diffusion to anomalous transport thus overlapping of different types of phenomena, potentially including drug diffusion and polymer swelling.

Table 4: Drug release kinetic paramete	ers of	microspheres.
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Batch	Zero Order		First Order		Matrix		Korsemeyer Peppas			Hixon- Crowel	
Code	(K)	(R ²)	(K)	(R ²)	(K)	(R ²)	(K)	(R ²)	(n)	(K)	(R ²)
A1	8.447	0.914	-0.166	0.994	24.71	0.994	22.68	0.995	0.539	-0.042	0.990
A2	7.257	0.950	-0.120	0.993	21.09	0.988	17.06	0.996	0.600	-0.033	0.992
A3	6.432	0.966	-0.975	0.992	18.62	0.980	14.14	0.996	0.629	-0.028	0.994
B1	7.708	0.981	-0.139	0.977	22.19	0.968	14.77	0.994	0.692	-0.037	0.992
B2	6.526	0.984	-0.109	0.993	18.76	0.965	11.48	0.997	0.734	-0.028	0.996
B3	5.725	0.984	-0.081	0.989	16.43	0.959	9.042	0.996	0.785	-0.024	0.996
C1	9.244	0.891	-0.206	0.985	27.14	0.996	25.75	0.998	0.524	-0.050	0.993
C2	8.511	0.931	-0.166	0.991	24.84	0.993	19.69	0.998	0.615	-0.043	0.995
C3	7.633	0.968	-0.133	0.994	22.08	0.978	15.51	0.997	0.668	-0.036	0.994

For the structural, crystal and physical state characterization, DSC studies of Azithromycin, Ethyl cellulose, their physical mixture and microspheres were carried out. The DSC thermograms are given Figure 6, 7, 8.And 9 show the DSC curves of Azithromycin, ethyl cellulose, physical mixture and microspheres (C1) respectively. DSC curve of Azithromycin shows a single endothermic peak at 121 °c, due to melting of the drug. Optimized formulation C1 which contains Azithromycin and ethyl cellulose, the thermogram indicates characteristic peaks for melting of Azithromycin at 121 °c. This indicates absence of drug - polymer interactions. This observation further supports the IR spectroscopy results.



Figure-6: DSC Thermogram of Azithromycin



Figure-7: DSC Thermogram of Ethyl Cellulose



Figure-8: DSC Thermogram of Physical mixture of Azithromycin+Ethyl Cellulose



Figure-9: DSC Thermogram of Microspheres (C1)

Figure 10, 11, 12, 13 represents the XRD diffraction pattern of Azithromycin, Ethyl cellulose, their physical mixture and microspheres (C1). The XRD scan of Azithromycin showed intense peaks of crystallinity. Diffractogram of azithromycin showed high intensity peaks between 20 of $10-20^{\circ}$ values demonstrating the crystalline nature of drug. No intense peaks were observed in diffractogram of ethyl cellulose which indicates amorphous nature. The XRD pattern of formulation exhibited halo pattern with less intense and denser peaks compared to plain Azithromycin. This indicated that Azithromycin is dispersed at the molecular level in the blend of polymeric matrix.



Figure-10: XRD pattern of Azithromycin





Figure-12: XRD pattern of Physical mixture



Figure-13: XRD pattern of microspheres (C1)

Figure No: 14, 15 shows the SEM photographs of various images of prepared formulation. SEM photographs showed that the microspheres were spherical in nature and had a smooth surface. SEM photographs revealed the absence of crystals of drug on the surface of microspheres and uniform distribution of the drug within the microspheres.

Accelerated stability studies (AST) was carried for optimized batch (C1) by exposing it to 40 $^{\circ}$ C \pm 2 $^{\circ}$ C, 75% \pm 5% RH for one month and analyzed the samples at the interval of 7,14,21,30 days and the samples was analyzed for drug content and *in-vitro* dissolution study. The stability studies show that there were no significant changes in observed drug content and percent cumulative drug release¹⁸.



Figure-14: External surface of microsphere



Figure-15: Whole image of microsphere

Table 5: Stability studies parameters

Paramotors	Days						
Farameters	7	14	21	30			
Drug content	74.41 ±	73.95 ±	74.52 ±	74.14 ±			
(%)	1.32	1.30	1.31	1.34			
In- vitro dissolution	80.11 ±	79.34 ±	79.55 ±	80.55 ±			
study	0.24	0.23	0.21	0.22			

5. CONCLUSION

From the investigation carried out and results obtained, it was observed that the % of drug released from microspheres was sustained. As the GI side effects of Azithromycin are related to its high dose which can be minimized by formulating as microspheres. It would also helps to improve bioavailability because of absorption window and microencapsulation helps to mask the bitter taste of drug. Hence from this investigation, we can propose that the objective of the study was achieved.

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